

# Image analysis and Pattern Recognition

## Lecture 1 : image pre-processing

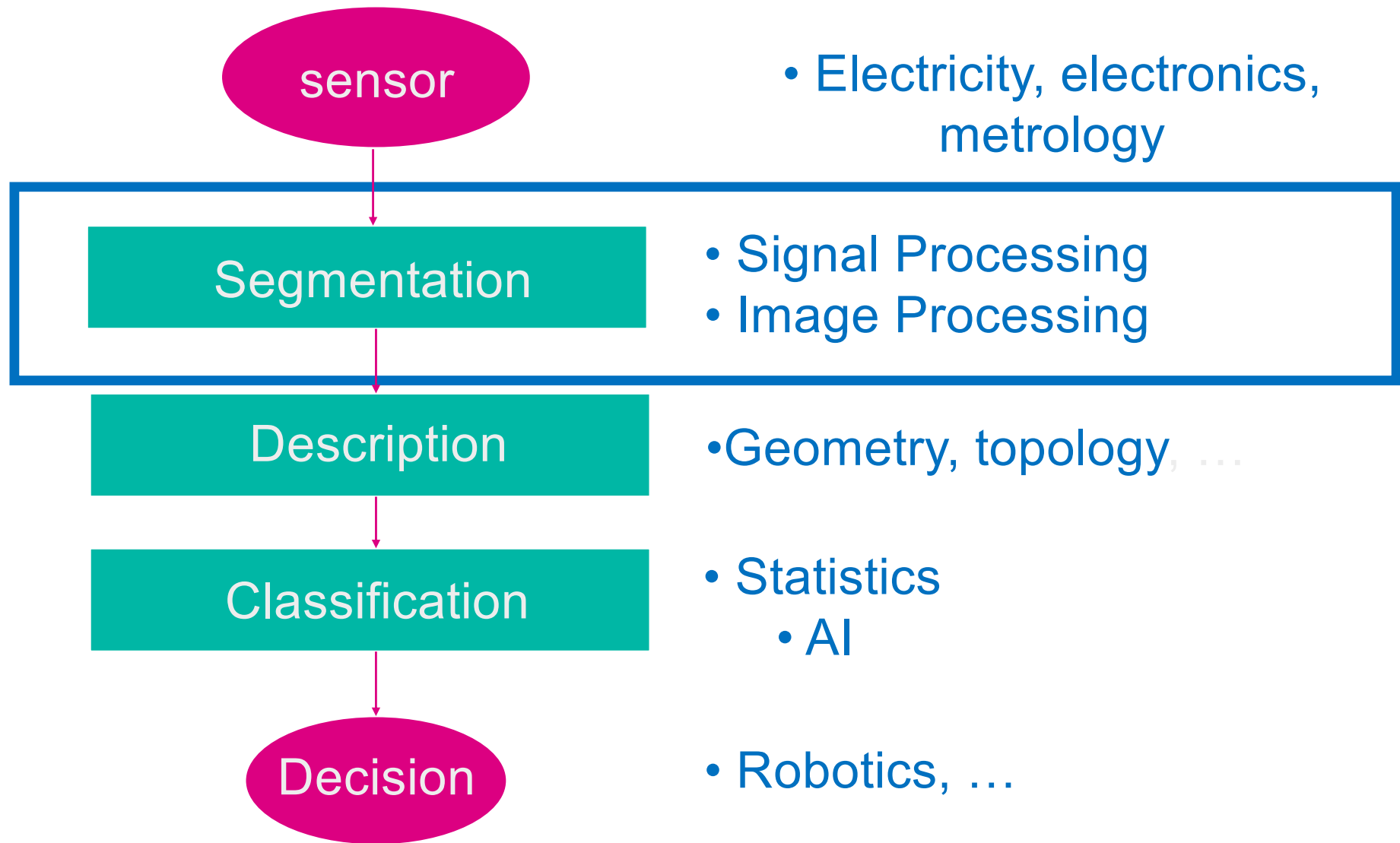
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**EPFL**



- Chapter 1 : Image Segmentation

- Digital images, properties & consequences of those properties
- Pre-processing
  - Histogram Equalization
  - Denoising and image restoration
- Segmentation:
  - Contour-based approach
  - Region-based approach
  - Mathematical Morphology
  - (Hough Transform)
- Some examples

Lecture 1

Lecture 2



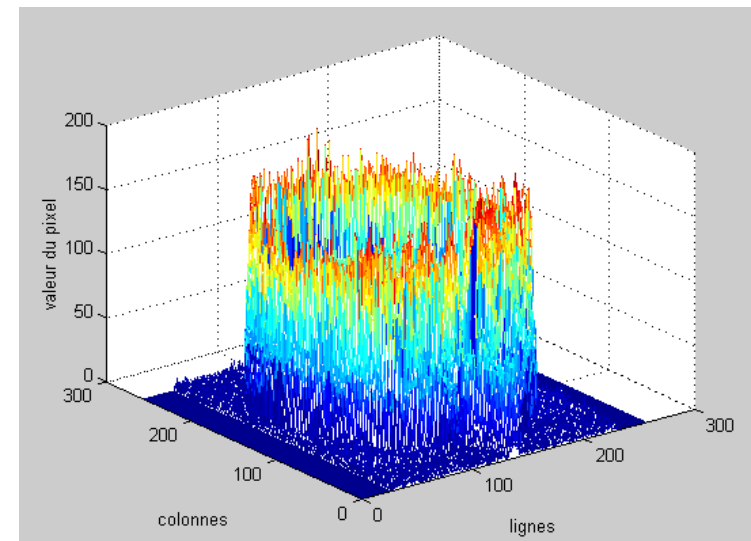
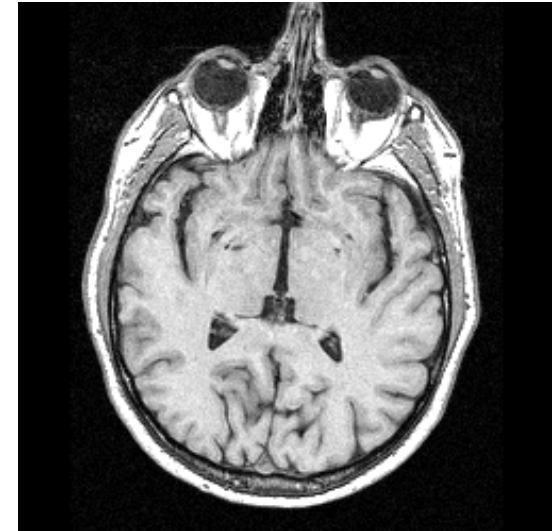
- An **image** is a function of (at least) 2 spatial variables :

$$f : \mathbb{R}^m \rightarrow \mathbb{R}^n, \vec{x} \mapsto \vec{y} = f(\vec{x})$$

- 2D Images:  $m = 2$ , i.e.  $\vec{x} = (x, y)$
- Monochromatic images:  $n = 1$
- Digital images: discrete domain:

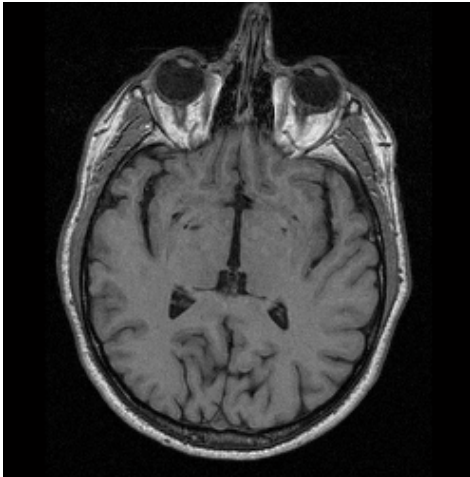
$$f : \mathbb{N}^m \rightarrow \mathbb{R}^n$$

- *The points are pixels (voxels in 3D)*

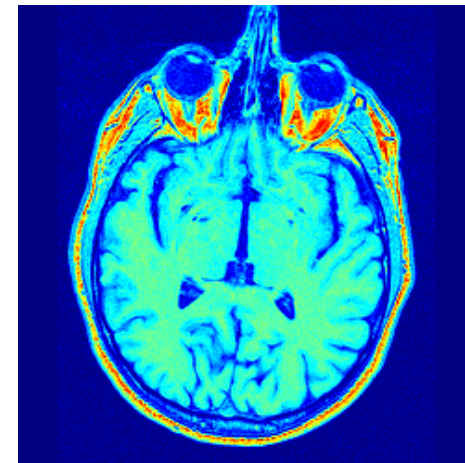




- Monochromatic images: 1 scalar / pixel
  - Often displayed as grey levels
  - Choice of other color lookup tables (CLUT) : « false colors »



Valeur	R	G	B
0	0/255	0/255	0/255
1	1/255	1/255	1/255
2	2/255	2/255	2/255
3	3/255	3/255	3/255
...	...	...	...
255	255/255	255/255	255/255



Valeur	R	G	B
0	0	0	0.5
1	0	0	0.52
...	...	...	...
150	1	0.34	0
...	...	...	...
255	0.5	0	0

- Multi-spectral images:
  - 1 vector/pixel
    - Example : color images
      - *Each pixel has three color components, in a given color space*
      - *Example : display on a screen: RGB*
      - *Example : TV diffusion: YUV ou YIU (Y=luminance)*

$$\begin{pmatrix} Y \\ I \\ Q \end{pmatrix} = \begin{pmatrix} 0.299 & 0.587 & 0.114 \\ 0.596 & -0.275 & -0.321 \\ 0.212 & -0.523 & 0.331 \end{pmatrix} \begin{pmatrix} R \\ G \\ B \end{pmatrix}$$

- Luminance is a good component to identify objects



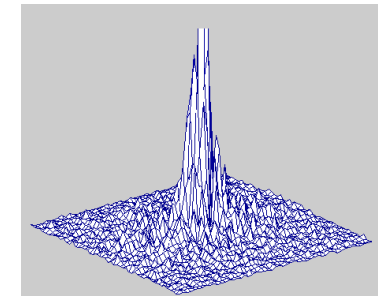
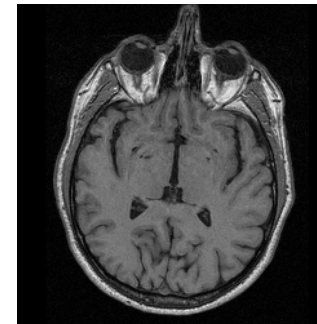
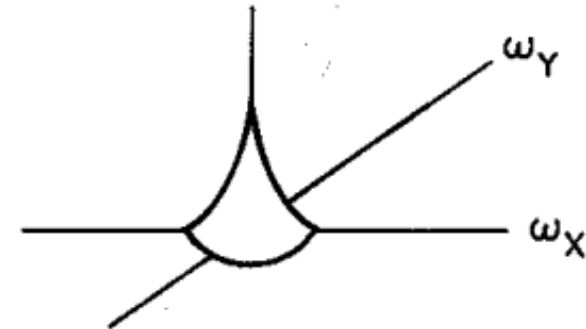
- Let  $f(x,y)$  be a 2D image
  - Its **Fourier Transform** is

$$F(f_x, f_y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(x, y) e^{-j2\pi(f_x x + f_y y)} dx dy$$

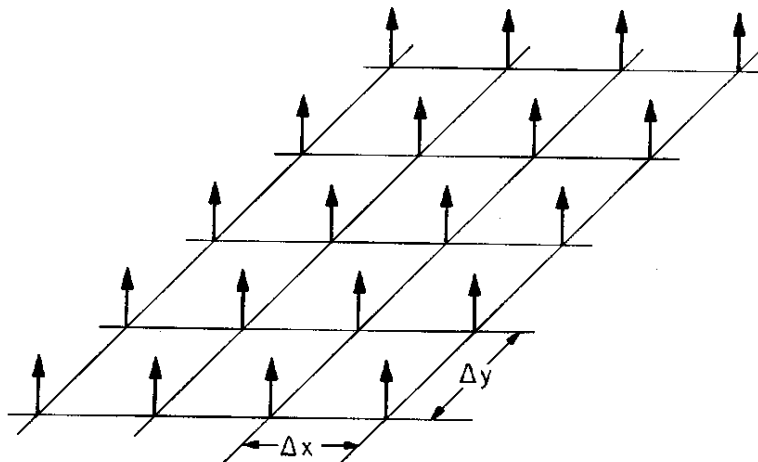
- It is separable :

$$F_y(f_x, y) = \int_{-\infty}^{\infty} f(x, y) e^{-j2\pi f_x x} dx$$

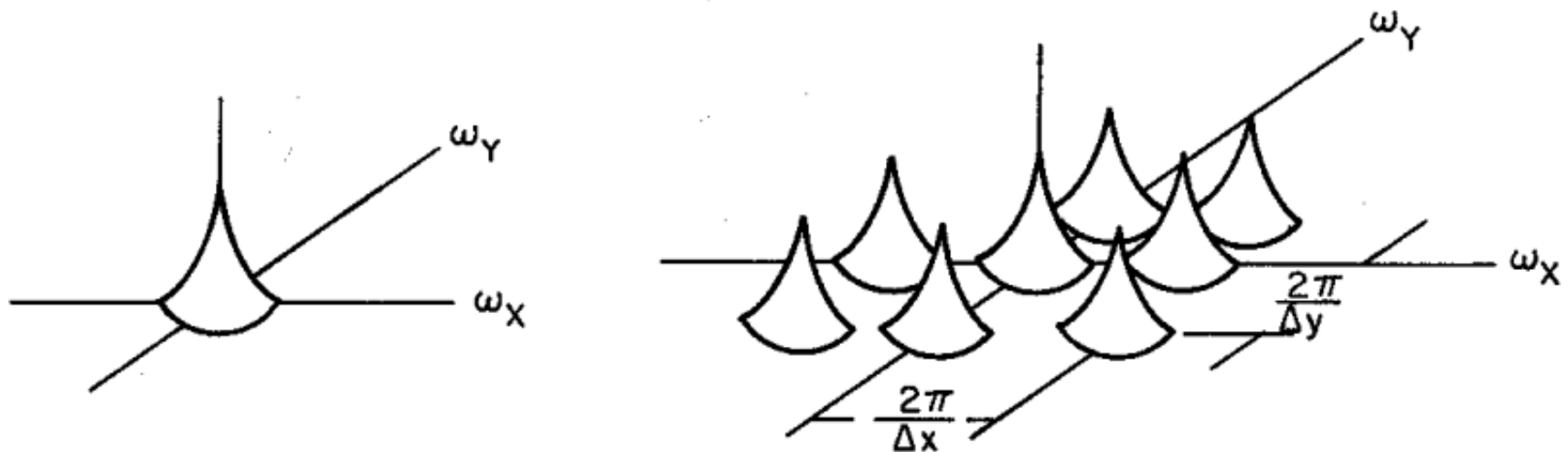
$$F(f_x, f_y) = \int_{-\infty}^{\infty} F_y(f_x, y) e^{-j2\pi f_y y} dy$$



- **Sampling** a continuous function (image)  $f(x,y)$  means taking samples at every  $\Delta x$  and  $\Delta y$
- $f_{ex}$  and  $f_{ey}$  are the vertical and horizontal sampling frequencies, respectively
- Mathematically, this means multiplying the analog image  $f(x,y)$  by **a grid of Dirac impulses**

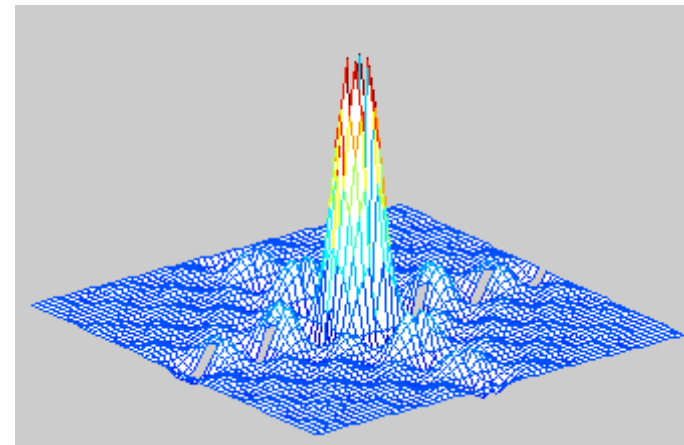
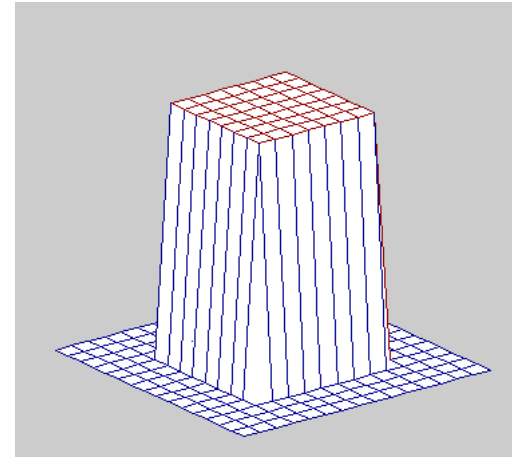


- Thus, the **spectrum** of the sampled image can be obtained by a convolution of the spectrum of the analog image with the FT of the grid of Dirac impulses:

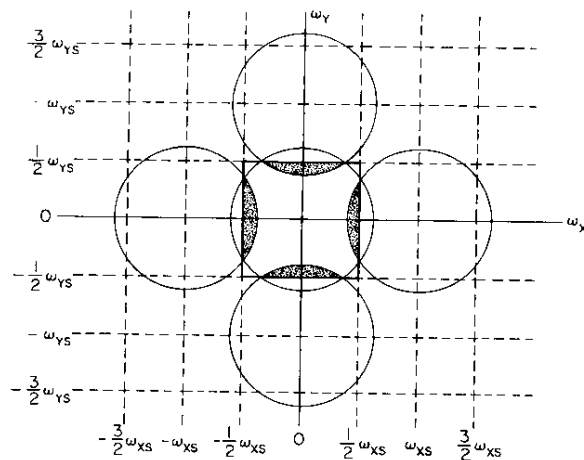


- From the spectrum of the sampled image, one can try to **reconstruct** the original image by low pass filtering:
  - Multiply the spectrum by a **rectangle function** in 2D
  - Convolve the sampled image by a signal of type  $\sin(x)/x$  in 2D

$$R(x, y) = \frac{K \omega_{xL} \omega_{yL}}{\pi^2} \frac{\sin(\omega_{xL} x)}{\omega_{xL} x} \frac{\sin(\omega_{yL} y)}{\omega_{yL} y}$$



- Practical implication: **scale change** (« zoom »)
  - Up-sampling : interpolation by  $R(x,y)$
  - Down-sampling: low-pass filtering + interpolation, otherwise aliasing



Aliasing



Originale Image

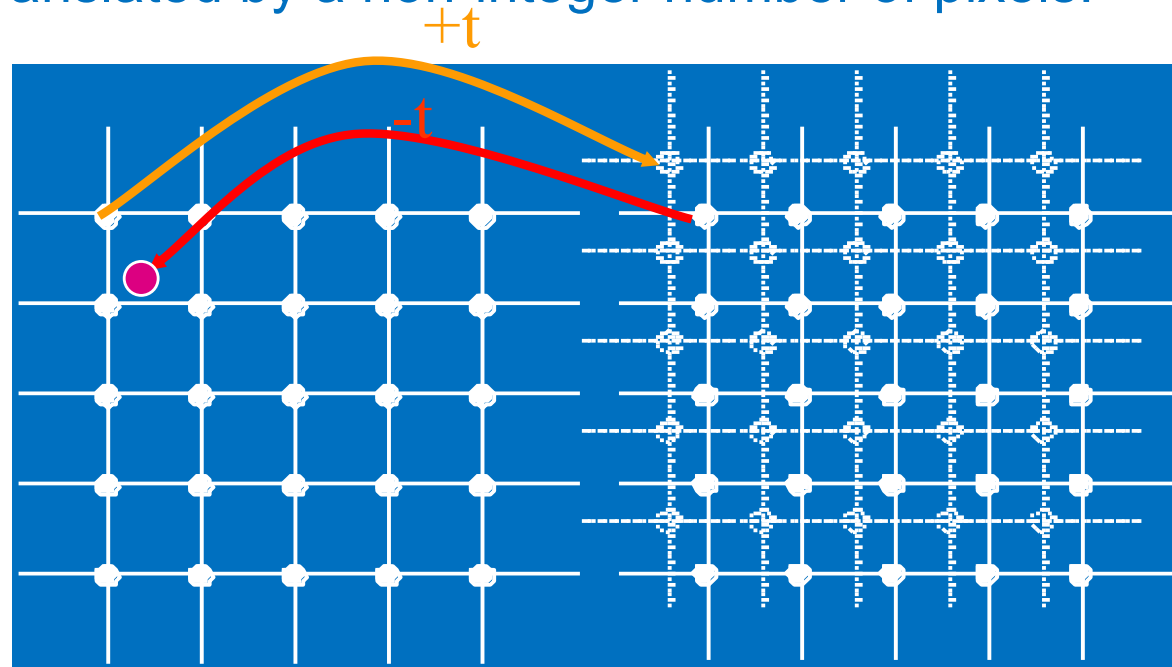


Aliasing

- Following the same considerations, it is possible to perform **geometrical operations** on images, as a pre-processing step:
  - **translation** : thanks to interpolation, it is possible to reconstruct an image translated by a non-integer number of pixels:

$$\begin{pmatrix} x \\ y \end{pmatrix} = \begin{pmatrix} u \\ v \end{pmatrix} + \begin{pmatrix} t_x \\ t_y \end{pmatrix}$$

$$\begin{pmatrix} u \\ v \end{pmatrix} = \begin{pmatrix} x \\ y \end{pmatrix} - \begin{pmatrix} t_x \\ t_y \end{pmatrix}$$



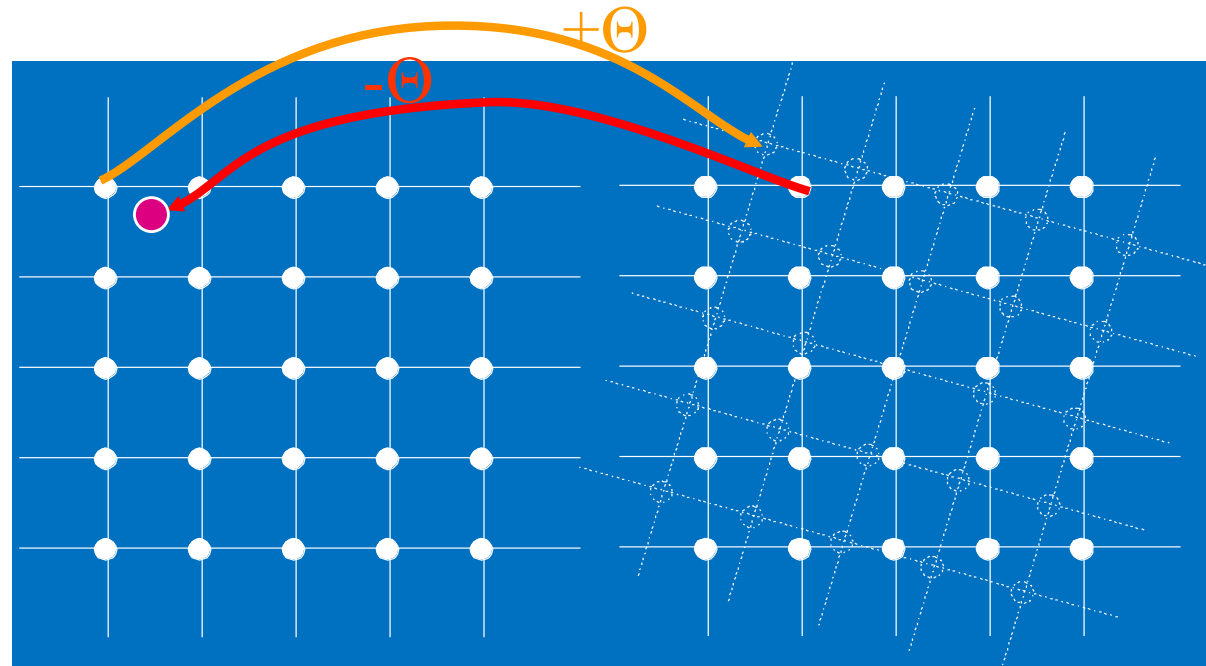
- **Inverse translation + interpolation**



- Other operations of the same type:
  - **rotation** : idem

$$\begin{pmatrix} x \\ y \end{pmatrix} = \begin{pmatrix} \cos \theta & -\sin \theta \\ \sin \theta & \cos \theta \end{pmatrix} \begin{pmatrix} u \\ v \end{pmatrix}$$

$$\begin{pmatrix} u \\ v \end{pmatrix} = \begin{pmatrix} \cos \theta & \sin \theta \\ -\sin \theta & \cos \theta \end{pmatrix} \begin{pmatrix} x \\ y \end{pmatrix}$$



- *rotation inverse + interpolation*
- And similarly for all the possible **geometrical transformations**

- More generally:
  - Linear transformations :

$$\begin{pmatrix} u \\ v \\ 1 \end{pmatrix} = \begin{pmatrix} a_1 & a_2 & a_0 \\ b_1 & b_2 & b_0 \\ 0 & 0 & 1 \end{pmatrix} \begin{pmatrix} x \\ y \\ 1 \end{pmatrix}$$

Translation :  $a_0 = -t_x, a_1 = 1, a_2 = 0, b_0 = -t_y, b_1 = 0, b_2 = 1$

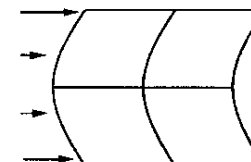
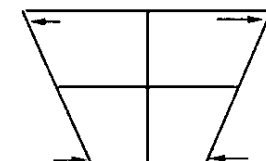
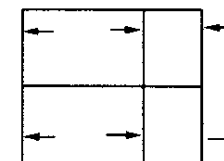
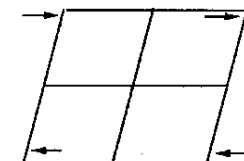
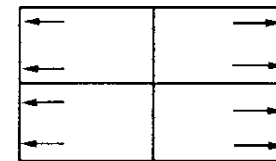
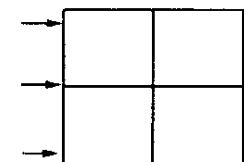
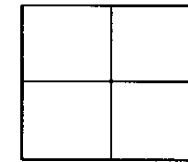
Rotation :  $a_0 = 0, a_1 = \cos \theta, a_2 = \sin \theta, b_0 = 0, b_1 = -\sin \theta, b_2 = \cos \theta$

Zoom :  $a_0 = 0, a_1 = 1/s, a_2 = 0, b_0 = 0, b_1 = 0, b_2 = 1/s$

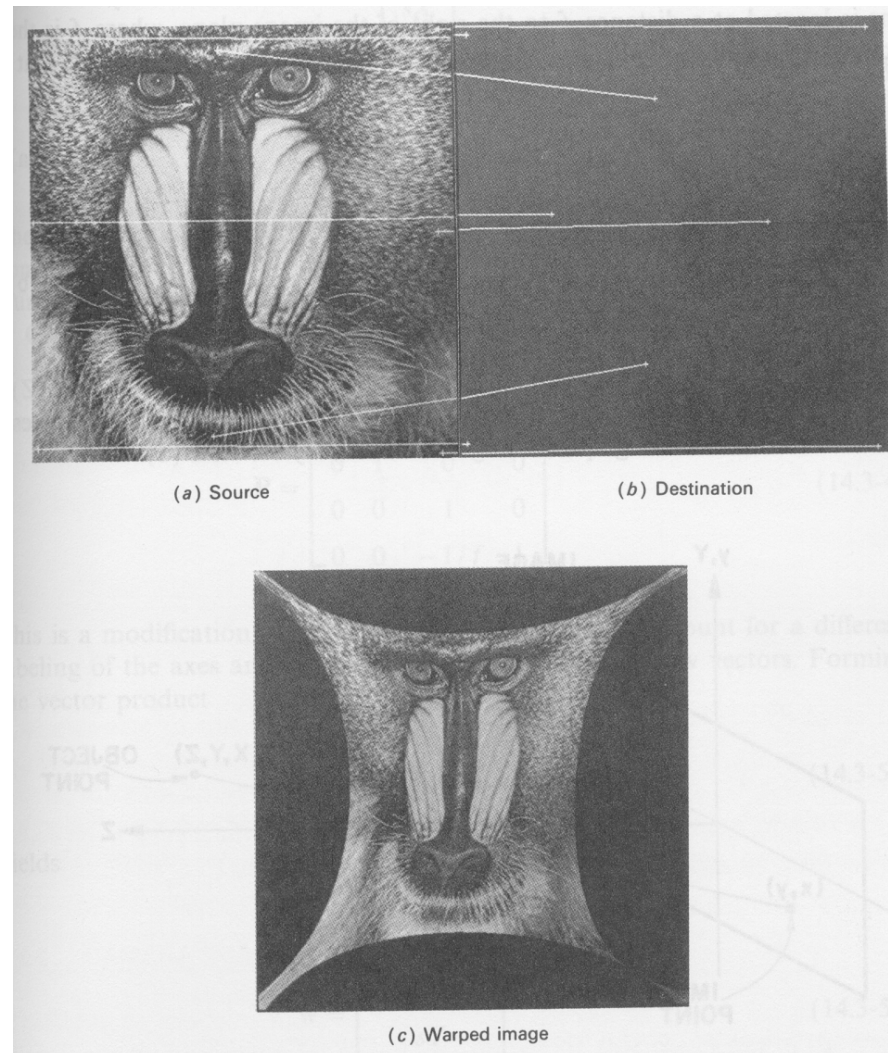
- Other geometrical transformations (non-linear):
  - Polynomial deformation
    - *Ex: order 2*

$$u = a_0 + a_1x + a_2y + a_3x^2 + a_4xy + a_5y^2$$

$$v = b_0 + b_1x + b_2y + b_3x^2 + b_4xy + b_5y^2$$

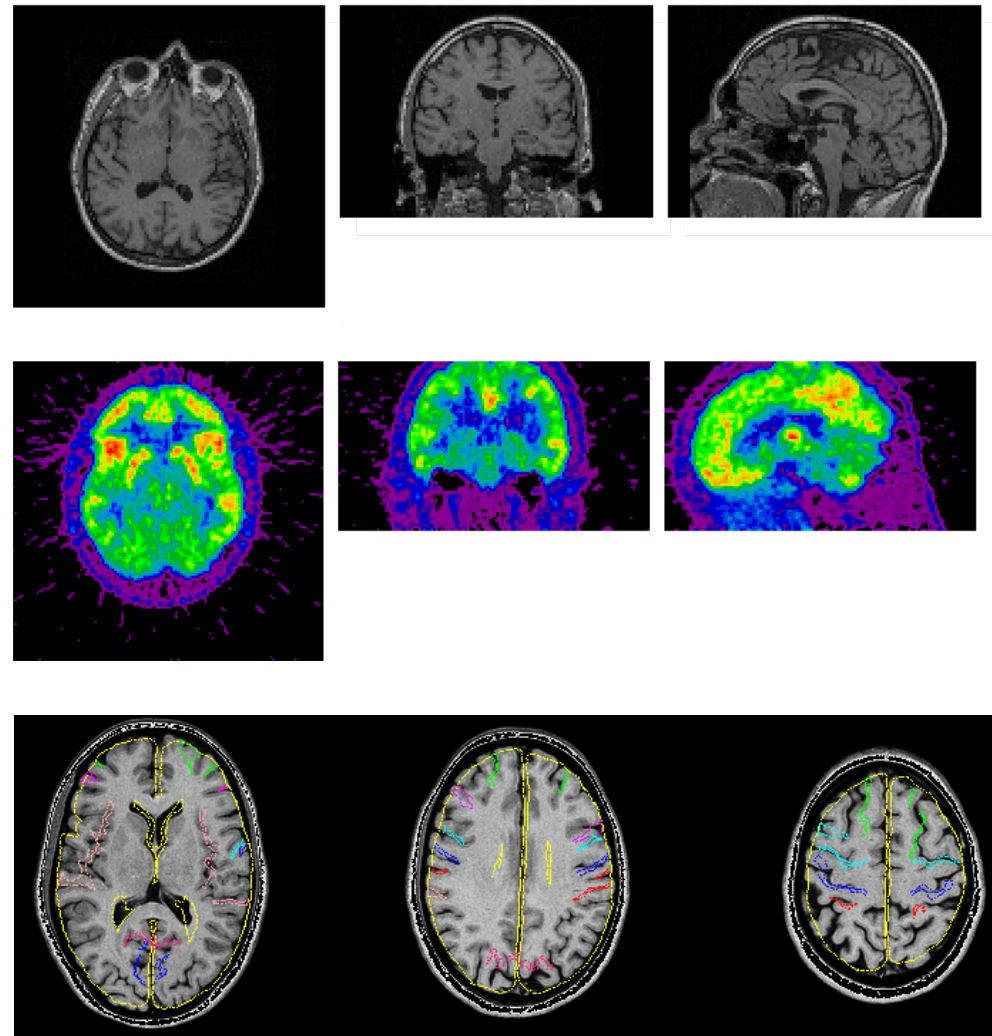


- Example of polynomial transformation

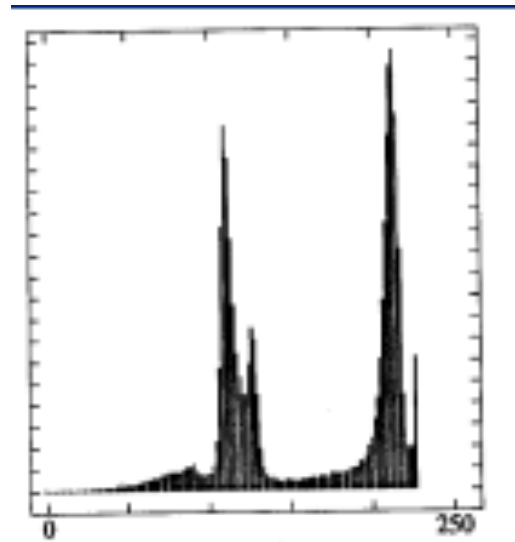
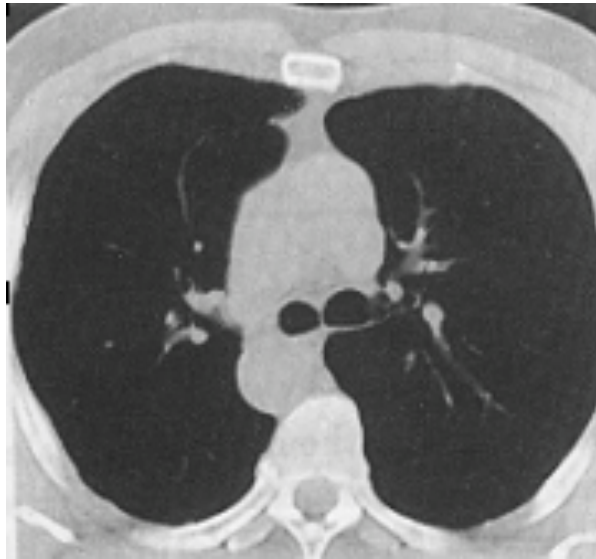


- Examples in **medical imaging**

- compensation of the difference in position between two patients
  - *rotation-translation*
- **Registration** in functional MRI
  - *rotation-translation*
- **Registration** between different patients
  - *Complex non-rigid registration (polynomial)*

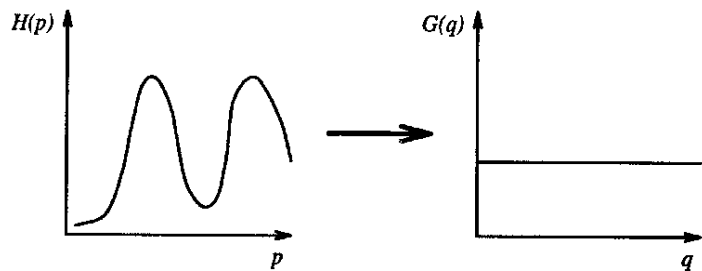


- Let us observe the histogram of the CT image



- Goal: create an image with a **uniform histogram**, by a transformation  $q=T(p)$

$$\sum_i G(q_i) = \sum_i H(p_i) \text{ et } G(q_i) = \frac{N^2}{q_k - q_0}$$



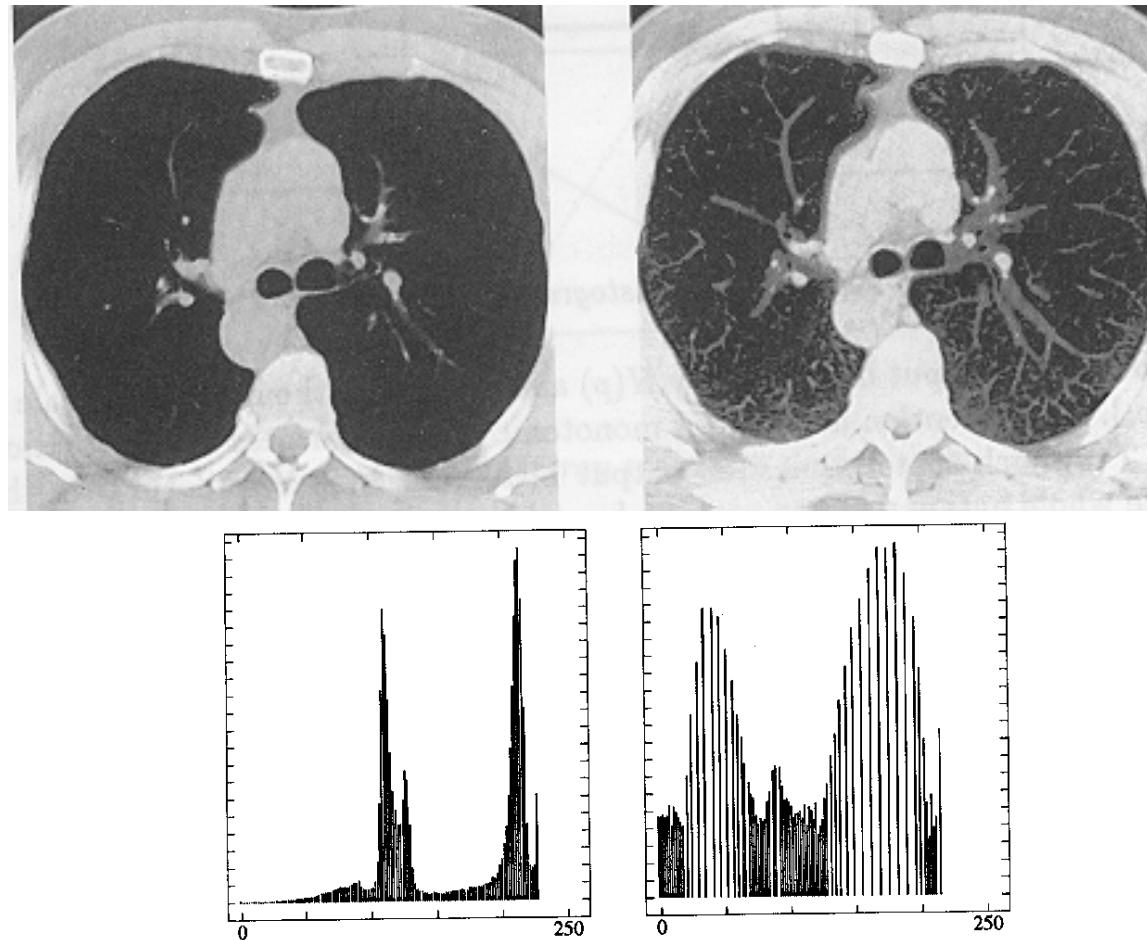
$$\int_{q_0}^q \frac{N^2}{q_k - q_0} ds = \frac{N^2}{q_k - q_0} (q - q_0) = \int_{p_0}^p H(s) ds$$

$$q = T(p) = \frac{q_k - q_0}{N^2} \int_{p_0}^p H(s) ds + q_0$$

$$q = T(p) = \frac{q_k - q_0}{N^2} \sum_{i=p_0}^p H(i) + q_0$$



- Example





- Vast topic!
- Source of **noise** in images:
  - All the interferences on the measurements (electrical, mechanical, ...)
  - Signal quantification
  - etc.
- Characteristics of the noise
  - **Random signal**
  - Often, in real situations, noise can be described as white, additive and Gaussian
  - But it may have sometimes other statistics (Reyleigh)
  - additive :  $y(t) = x(t) + n(t)$



- One can define the importance of the noise by the **signal to noise ratio**:

$$SNR = 10 \log \frac{P_S}{P_N} \quad [\text{dB}]$$

- If one can acquire several realization of the noisy signal, one can try to denoise it by exploiting the statistical properties (e.g. zero mean) of the noise.
  - Example : for an additive noise with zero mean, one can calculate the mean of the observations, which will reduce the noise:

If  $y(t) = x(t) + n(t)$

Then  $E(y(t)) = E(x(t) + n(t)) = E(x(t)) + E(n(t)) = E(x(t))$

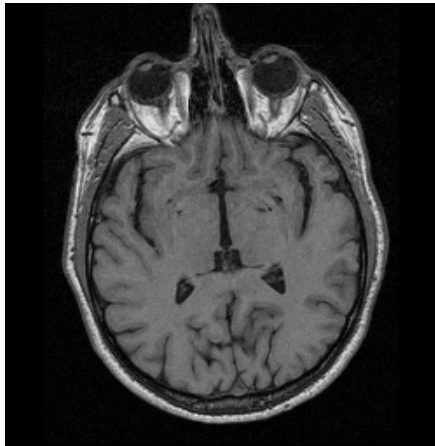
- If one has access to only one image: we have to use more general aspects:
  - Noise has a **large frequency spectrum**, containing also high frequencies (more than the images)
  - A **low-pass filtering** should reduce the noise
  - But there is a risk to alter the image as well!
- **Low-pass filtering:**
  - 2D convolution:  $G(i, j) = \sum_m \sum_n F(m, n) H(m - i, n - j)$
  - Some simple low-pass filters:

$$H = \frac{1}{9} \begin{bmatrix} 1 & 1 & 1 \\ 1 & 1 & 1 \\ 1 & 1 & 1 \end{bmatrix}$$

$$H = \frac{1}{10} \begin{bmatrix} 1 & 1 & 1 \\ 1 & 2 & 1 \\ 1 & 1 & 1 \end{bmatrix}$$

$$H = \frac{1}{16} \begin{bmatrix} 1 & 2 & 1 \\ 2 & 4 & 2 \\ 1 & 2 & 1 \end{bmatrix}$$

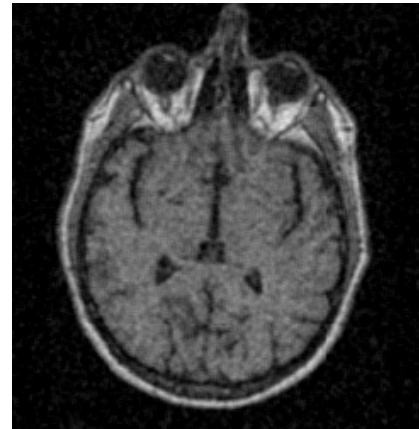
- Example :



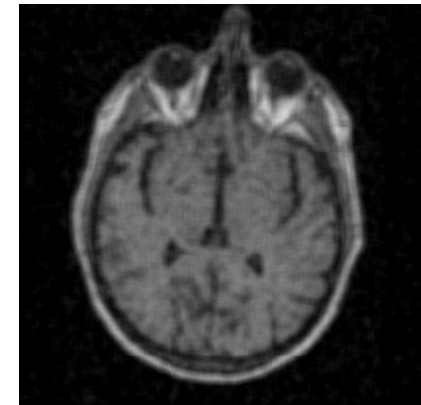
Original



With  
additive  
white  
Gaussian  
noise



Filtered  
(3x3 filter)



Filtered  
(5x5 filter)

- Sometimes the noise can be multiplicative
  - Noise depends on the intensity of the signal
  - example : nuclear medicine
- Then the model of the observed image is:
  - Initial image  $f_i(i,j)$  multiplied by the noise  $n(i,j)$

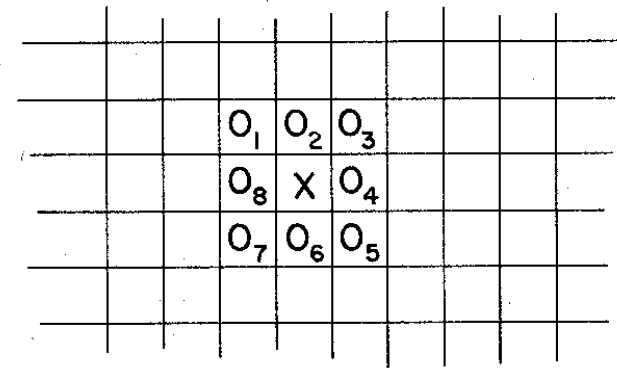
$$f_o(i, j) = f_i(i, j)n(i, j)$$

- By taking the logarithm, we can come back to an additive model, that we can filter

$$\log(f_o(i, j)) = \log(f_i(i, j)) + \log(n(i, j))$$

- **Linear filtering** works quite well for additive Gaussian noise
  - Even if it degrades the contours
- When the noise is of type “impulses”, we would need a very strong filter to suppress it, and the image would be very degraded
- **Non-linear techniques** often offer a good compromise between filtering power and respect of the image details

- Compare the pixel value with the mean of its neighbors
  - If the difference is greater than a certain threshold, the pixel is considered as noisy, and replaced by the mean of the neighbors
  - Can be seen as a conditional convolution by

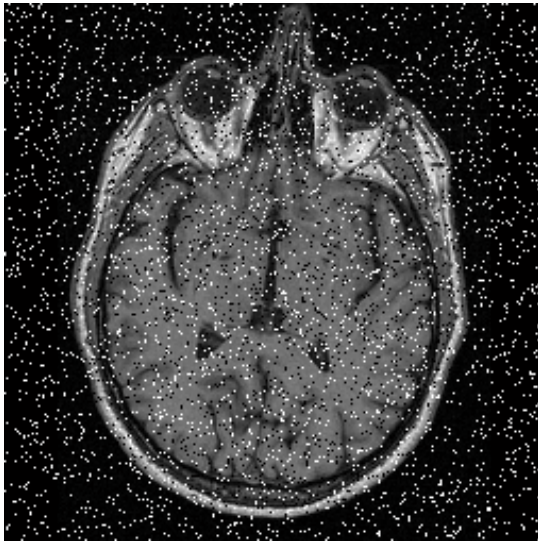


$$\text{IF } \left[ x - \frac{1}{8} \sum_{i=1}^8 O_i \right] > \epsilon \quad \text{THEN}$$

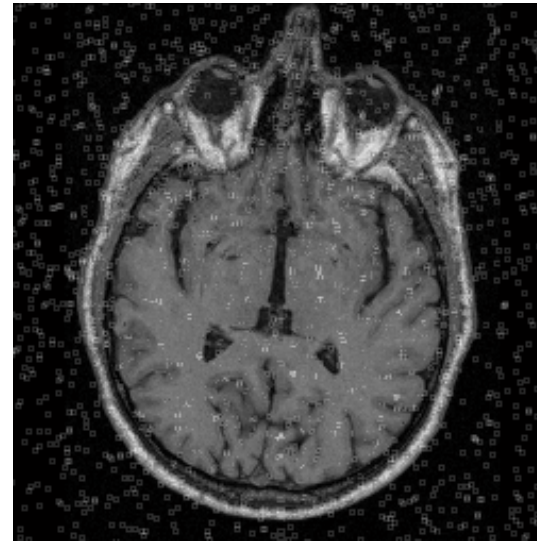
$$x = \frac{1}{8} \sum_{i=1}^8 O_i$$

$$H = \frac{1}{8} \begin{bmatrix} 1 & 1 & 1 \\ 1 & 0 & 1 \\ 1 & 1 & 1 \end{bmatrix}$$

- Example



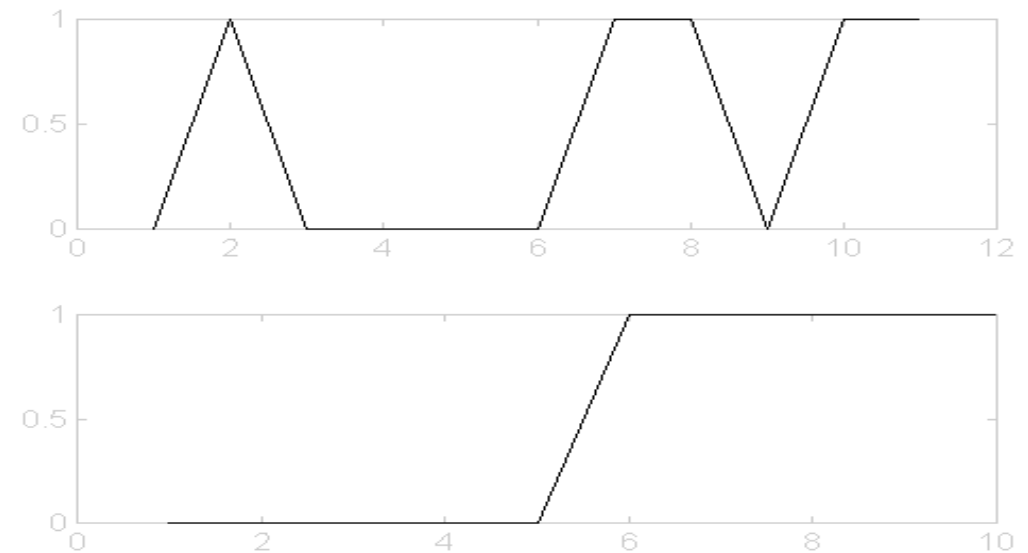
Noisy image  
« salt & pepper »



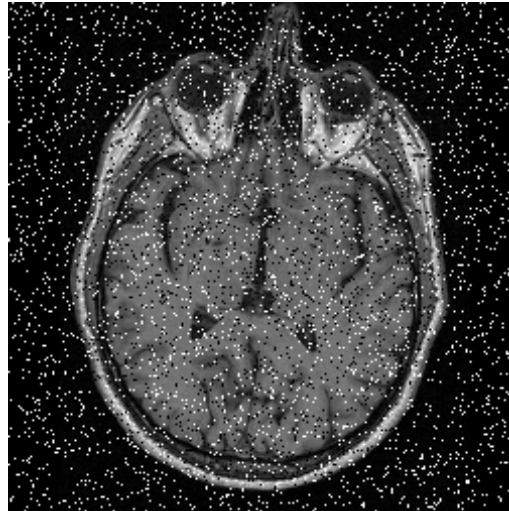
Denoised image



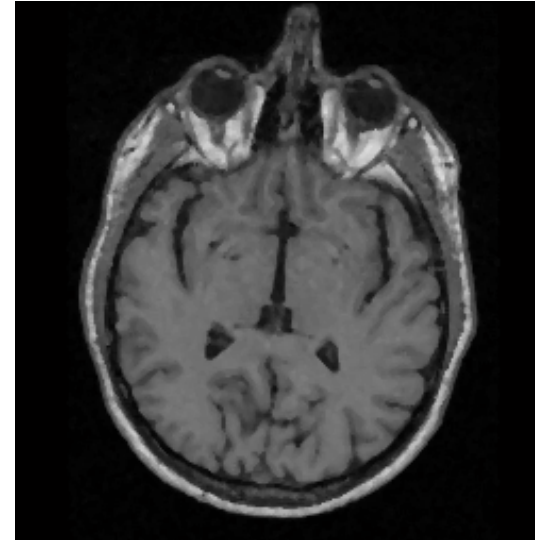
- Let us consider the neighbors of a pixel, on a neighborhood of size  $n \times n$
- Let us **sort the values** of those pixels in ascending order
- Let us set the **median** value of this list (not the mean) as the value of the current pixel
  - The median is the value of the middle element of the list
- Advantages :
  - Suppresses the small variations
  - **Keeps the contours**



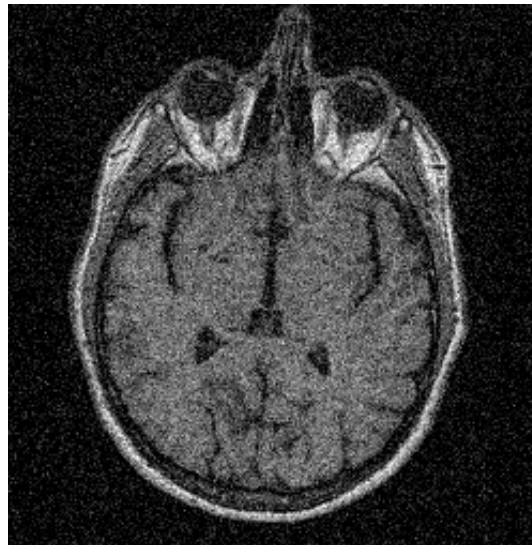
Noisy image  
« salt & pepper »



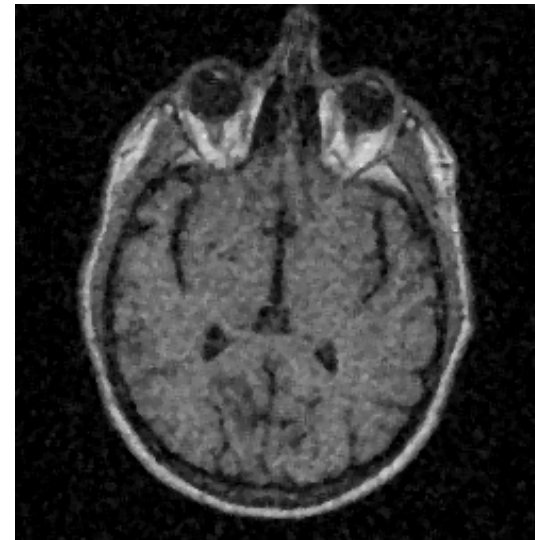
Denoised image  
« salt & pepper »



Noisy image  
Gaussian noise



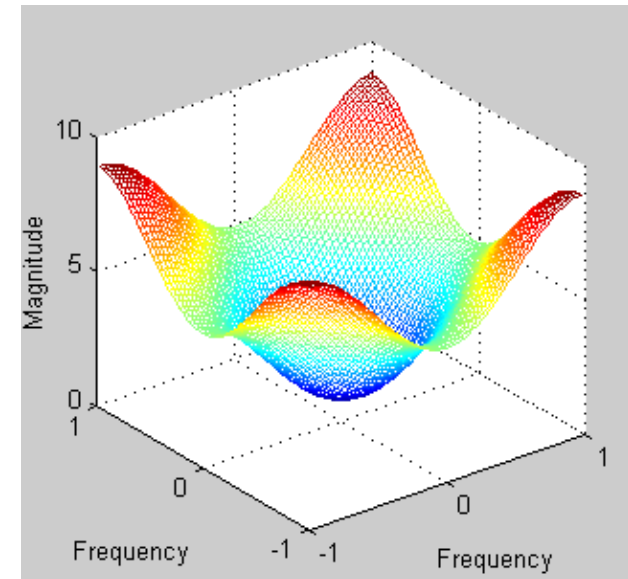
Denoised image  
Gaussian noise



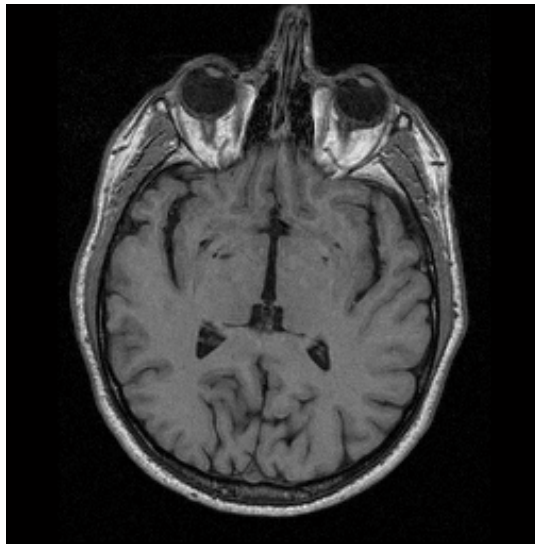
- General Principle:
  - Enhance the high frequencies
    - Filtering by a high pass filter, added to the original image
- Some examples of high pass filters:

$$H_1 = \begin{bmatrix} 0 & -1 & 0 \\ -1 & 5 & -1 \\ 0 & -1 & 0 \end{bmatrix} \quad H_2 = \begin{bmatrix} -1 & -1 & -1 \\ -1 & 9 & -1 \\ -1 & -1 & -1 \end{bmatrix}$$

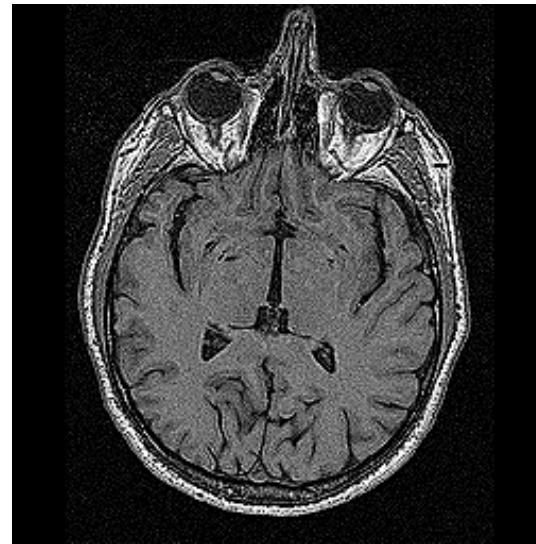
$$H_3 = \begin{bmatrix} 1 & -2 & 1 \\ -2 & 5 & -2 \\ 1 & -2 & 1 \end{bmatrix}$$



- Example : MRI



Original



Enhanced : filter  $H_1$

- Example : X ray



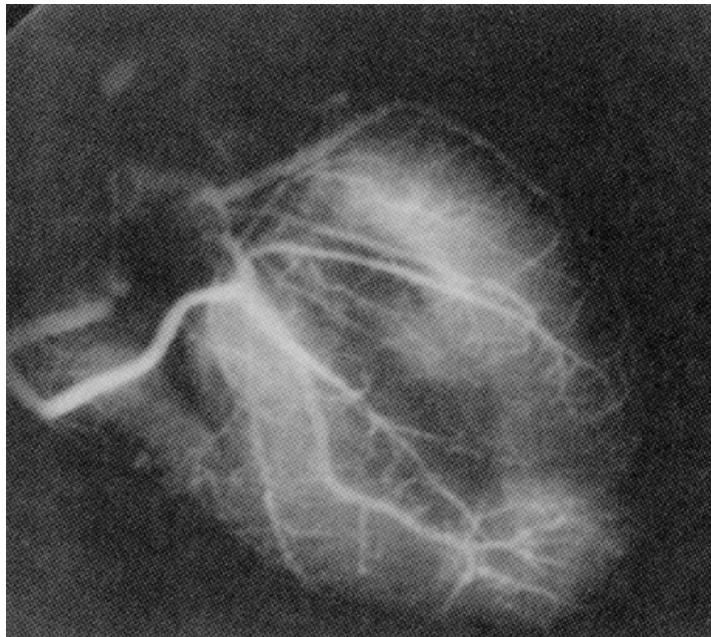
Original



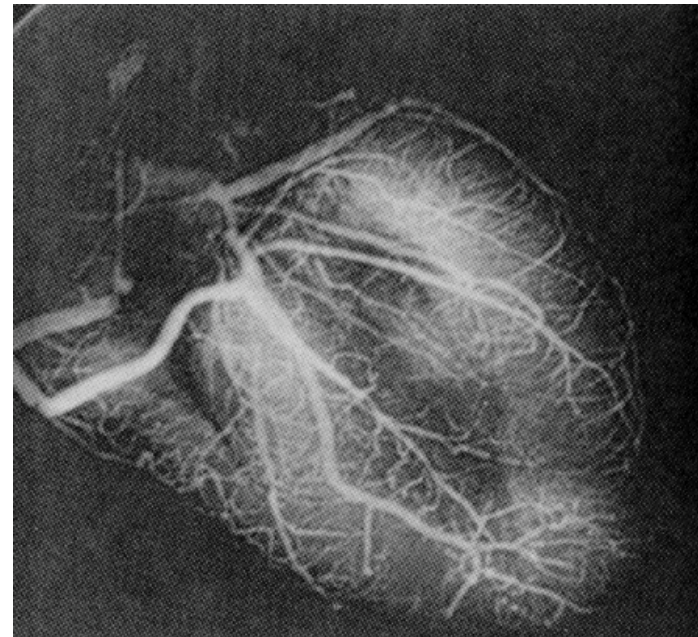
Enhanced : filter  $H_1$



- Example : DSA

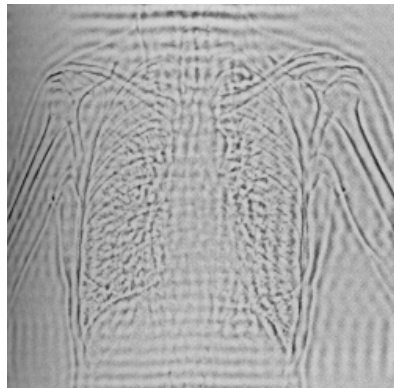


Original

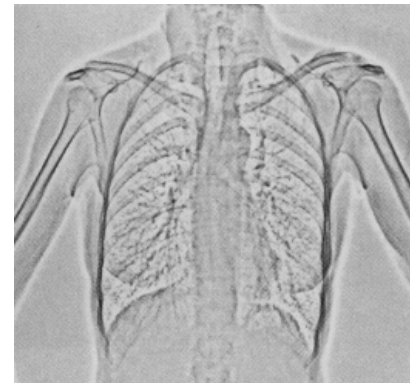


Enhanced : filter  $H_1$

- Contour Enhancement in the Fourier domain
  - Filtering by a high pass filter
  - Keep the original image and add the high pass component
  - **Warning**: do not use too strict filters, because of the ringing effect
  - Prefer a smooth filter like Butterworth



Too strict filter



Butterworth

- **Restoration** : invert non-wanted effects
- Typical application: **deconvolution**
  - Let us consider the ideal image  $f_i$  that has been degraded by an undesired (low pass) filtering effect
  - Let  $f_o$  be the observed image
  - Moreover, there is an additive noise  $n$ ,

$$f_o(x, y) = f_i(x, y) ** h_D(x, y) + n(x, y)$$

- **Goal** : try to **restore the initial image**, using a model for the original image and for the noise



- **Inverse filtering**: let us find a filter  $h_R$  that will best restore the image  $f_i$
- The restored image will thus be

$$\hat{f}_i(x, y) = f_o(x, y) ** h_R(x, y)$$

- By substitution in the previous equation, we get

$$\hat{f}_i(x, y) = [f_i(x, y) ** h_D(x, y) + n(x, y)] ** h_R(x, y)$$

- By FT:

$$\hat{F}_i(\omega_x, \omega_y) = [F_i(\omega_x, \omega_y)H_D(\omega_x, \omega_y) + N(\omega_x, \omega_y)]H_R(\omega_x, \omega_y)$$

- Thus,, the solution consists in taking a filter  $h_R$  with a frequency response inverse of that of  $h_D$  :

$$H_R(\omega_x, \omega_y) = \frac{1}{H_D(\omega_x, \omega_y)}$$

- The spectrum of the restored image is thus

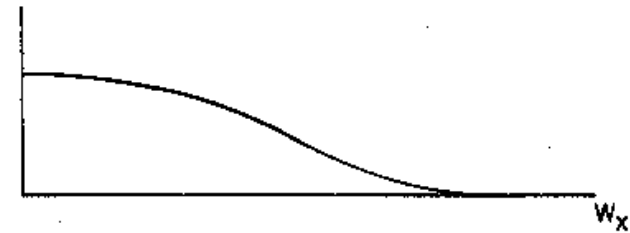
$$\hat{F}_i(\omega_x, \omega_y) = F_i(\omega_x, \omega_y) + \frac{N(\omega_x, \omega_y)}{H_D(\omega_x, \omega_y)}$$

- And by inverse FT, the restored image will be

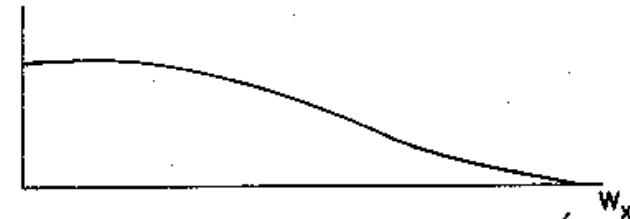
$$\hat{f}_i(x, y) = f_i(x, y) + \frac{1}{4\pi^2} \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} \frac{N(\omega_x, \omega_y)}{H_D(\omega_x, \omega_y)} e^{j(\omega_x x + \omega_y y)} d\omega_x d\omega_y$$

- Without noise, the restoration is perfect
- With noise, the error can be important:
  - Often  $h_D$  will be a low-pass filter (blur, ...)
  - Noise will thus be amplified

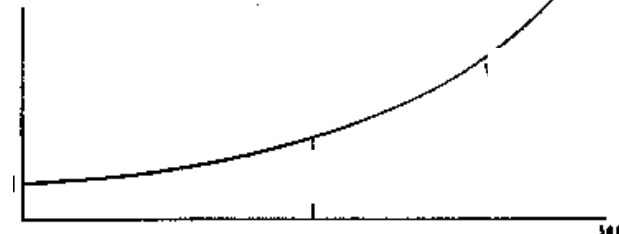
$$|F_i(\omega_x, 0)|$$



$$|H_D(\omega_x, 0)|$$



$$|H_R(\omega_x, 0)|$$



- Example



Original

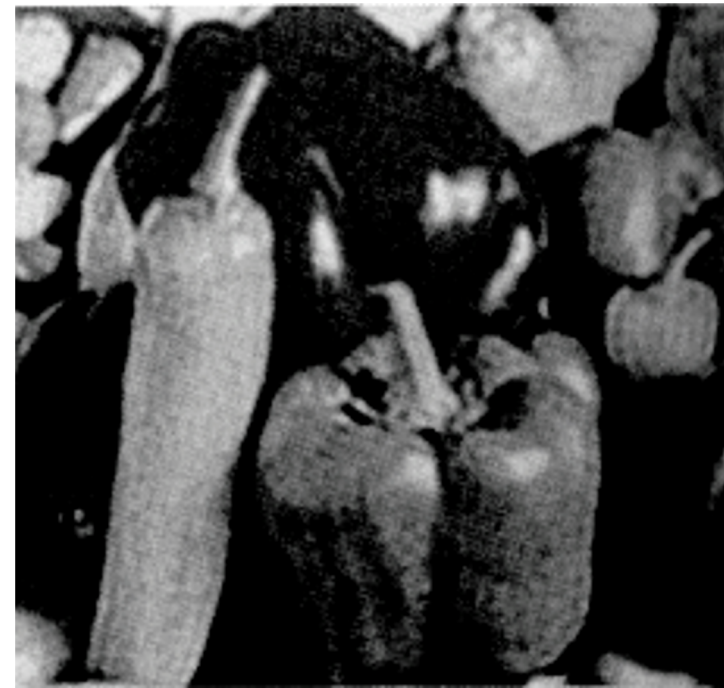


Blurred image  
(filtered)



Noisy and blurred

- Example (cont.)



Restoration of the blurred image   Restoration of the noisy blurred image

- The previous problem comes from the fact that the filter ignores the presence of noise in the
  - solution : Wiener filtering, that considers both a model of the image and of the noise
- Wiener filtering: hypotheses :
  - Images are 2D random variables, with zero mean (can be obtained by subtracting the mean to the images)
- Goal: find a filter  $h_R$  that will minimize the quadratic error

$$\varepsilon = E \left\{ \left[ f_i(x, y) - \hat{f}_i(x, y) \right]^2 \right\}$$

- Calculating the 1st derivative, the error is minimal when

$$E\left\{\left[f_i(x, y) - \hat{f}_i(x, y)\right]f_o(x', y')\right\} = 0$$

- By replacing  $\hat{f}_i$  by its value, we get

$$E\{f_i(x, y)f_o(x', y')\} = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} E\{f_o(i, j)f_o(x', y')\} h_R(x-i, y-j) didj$$

- The expectations of this products are the intercorrelation and the autocorrelation of the variables:

$$K_{f_i f_o}(x-x', y-y') = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} K_{f_o}(i-x', j-y') h_R(x-i, y-j) didj$$



$$K_{f_i f_o}(x - x', y - y') = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} K_{f_o}(i - x', j - y') h_R(x - i, y - j) di dj$$

- By FT, we obtain

$$H_R(\omega_x, \omega_y) = \frac{P_{f_i f_o}(\omega_x, \omega_y)}{P_{f_o}(\omega_x, \omega_y)}$$

$P_{f_i f_o}(\omega_x, \omega_y)$  is the power interspectrum

$P_{f_o}(\omega_x, \omega_y)$  is the power spectrum of  $f_o$

- When the noise is additive, we can write, by the Wiener-Kintchine theorems :

$$P_{f_o}(\omega_x, \omega_y) = |H_D(\omega_x, \omega_y)|^2 P_{f_i}(\omega_x, \omega_y) + P_N(\omega_x, \omega_y)$$

and

$$P_{f_o f_i}(\omega_x, \omega_y) = H_D^*(\omega_x, \omega_y) P_{f_i}(\omega_x, \omega_y)$$

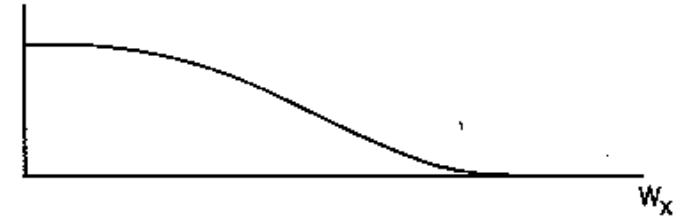
- And we finally obtain the **Wiener filter**, with frequency response:

$$H_R(\omega_x, \omega_y) = \frac{H_D^*(\omega_x, \omega_y)}{|H_D^*(\omega_x, \omega_y)|^2 + \frac{P_N(\omega_x, \omega_y)}{P_{f_i}(\omega_x, \omega_y)}}$$

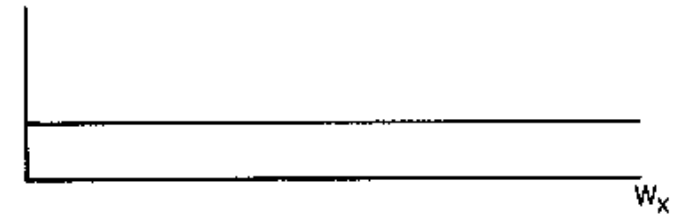
- Conclusions :

- The Wiener filter is a **adaptive band-pass filter**
- It behaves like the inverse filter at low frequencies and like a low-pass filter for high frequencies

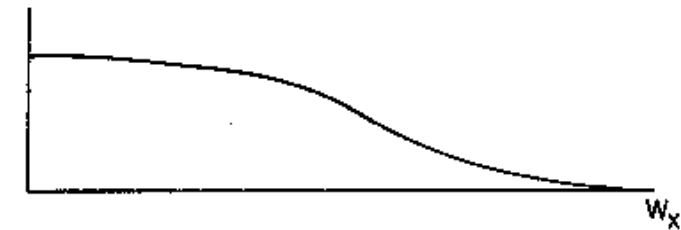
$$|P_{f_i}(\omega_x, 0)|$$



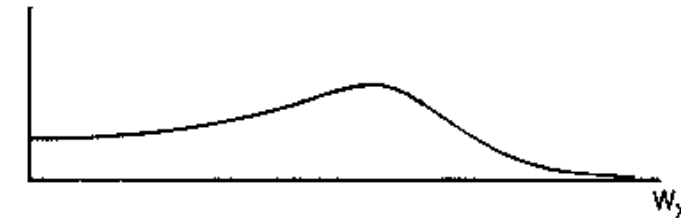
$$|P_N(\omega_x, 0)|$$



$$|H_D(\omega_x, 0)|$$



$$|H_R(\omega_x, 0)|$$



- Examples :



Motion blur



Restored Image

- Examples (cont.):



Out-of-focus blur



Restored image

- How to estimate  $h_D$  and the power spectrum of the noise?
  - $h_D$  is the impulse response of the system. Thus if we find in the image a place that should contain a punctual object, one can deduce  $h_D$
  - Similarly, a clear edge allows to evaluate the index response, integral of the impulse response
- For the power spectrum of the noise:
  - A uniform region in the image show the noise. The FT of its autocorrelation gives an estimation of the power spectrum of the noise

